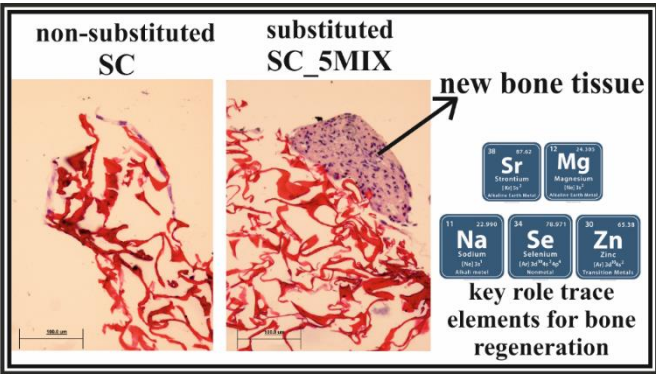


Manufacturing of biomimetic scaffolds for bone regeneration by using vat photopolymerization method – opportunities and challenges –

Antonia Ressler*, Erkka J. Frankberg, Roope Ohlsbom, Setareh Zakeri, Markus Hannula, Jari Hyttinen, Martin Schwentenwein, Susanna Miettinen, Erkki Levänen

AffordBoneS

Personalized and affordable multi-substituted calcium phosphate scaffolds



Objective 1/WP1
mCaP precipitation, design of mCaP scaffolds using CAD and scaffold fabrication

scaffold CAD model

substituted mCaP

CeraFab 7500 printer

Collaboration with : **LITHOZ**

The mCaP scaffold properties according to the bone tissue engineering requirements:
 -porosity: 50-90 %
 -pore size distribution: 100-500 μm
 -phase content: hydroxyapatite/tricalcium phosphate
 -mechanical properties required for bone augmentation

Objective 2/WP2
In vitro and *in vivo* osteogenic properties of mCaP scaffolds

***In vitro* cell culture in static and dynamic conditions**
 -live/ded assay, Cell Counting
 -quantitative reverse transcription polymerase chain reaction
 -immunocytochemical and immunohistochemical staining
 -histological staining

***In vivo* characterization during three months in rats**
 -micro-computed tomography
 -inflammation detection

Objective 3/WP3
Obtaining a demonstration of personalized mCaP scaffolds in collaboration with Planmecca

-obtaining CAD design according to the real patient cases provided by Planmecca
 -printing customized scaffolds on CaraFab 7500 using previously optimized printing parameters

Collaboration with : **PLANMECCA**



Prof. Erkki Levänen



Dr. Erkkka Frankberg



Prof. Susanna Miettinen



LITHOZ
Dr. Martin Schweintenwein



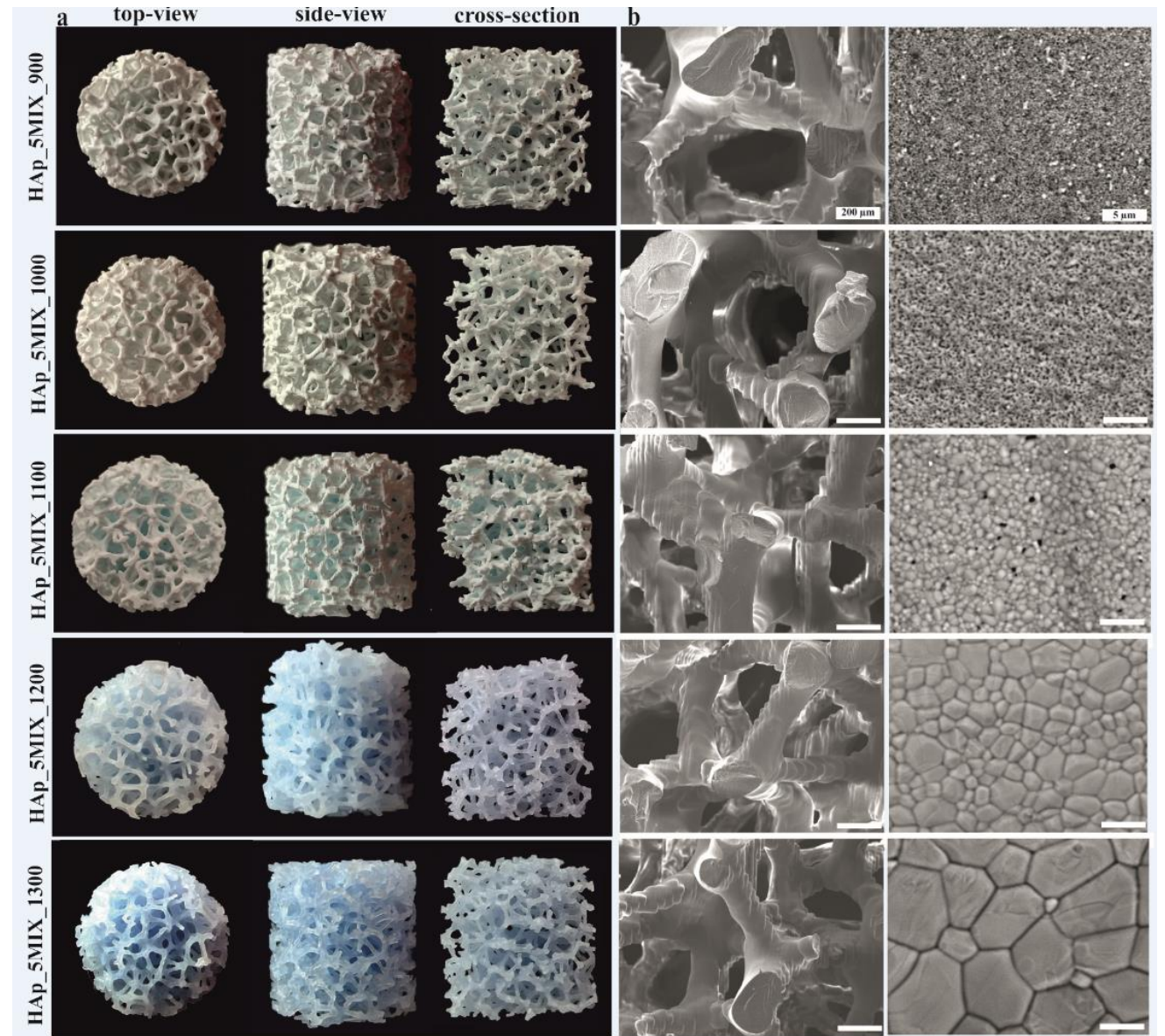
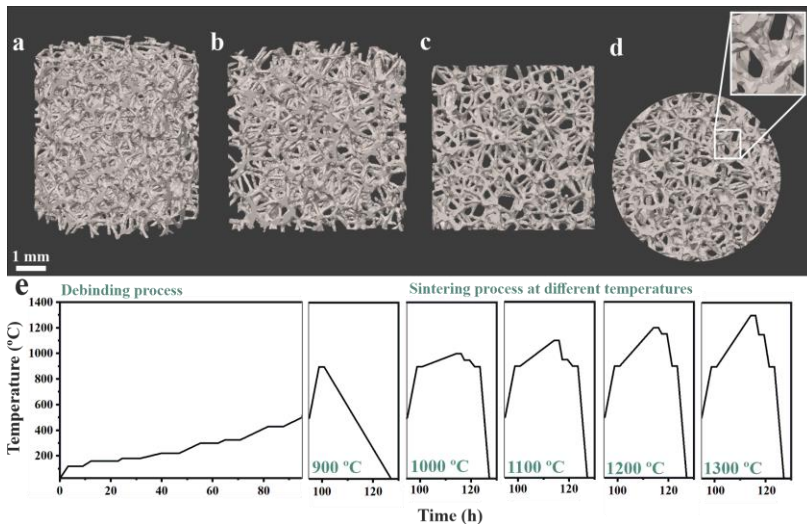
Pontus Degerlund
PLANMECCA



Dr. Antonia Ressler

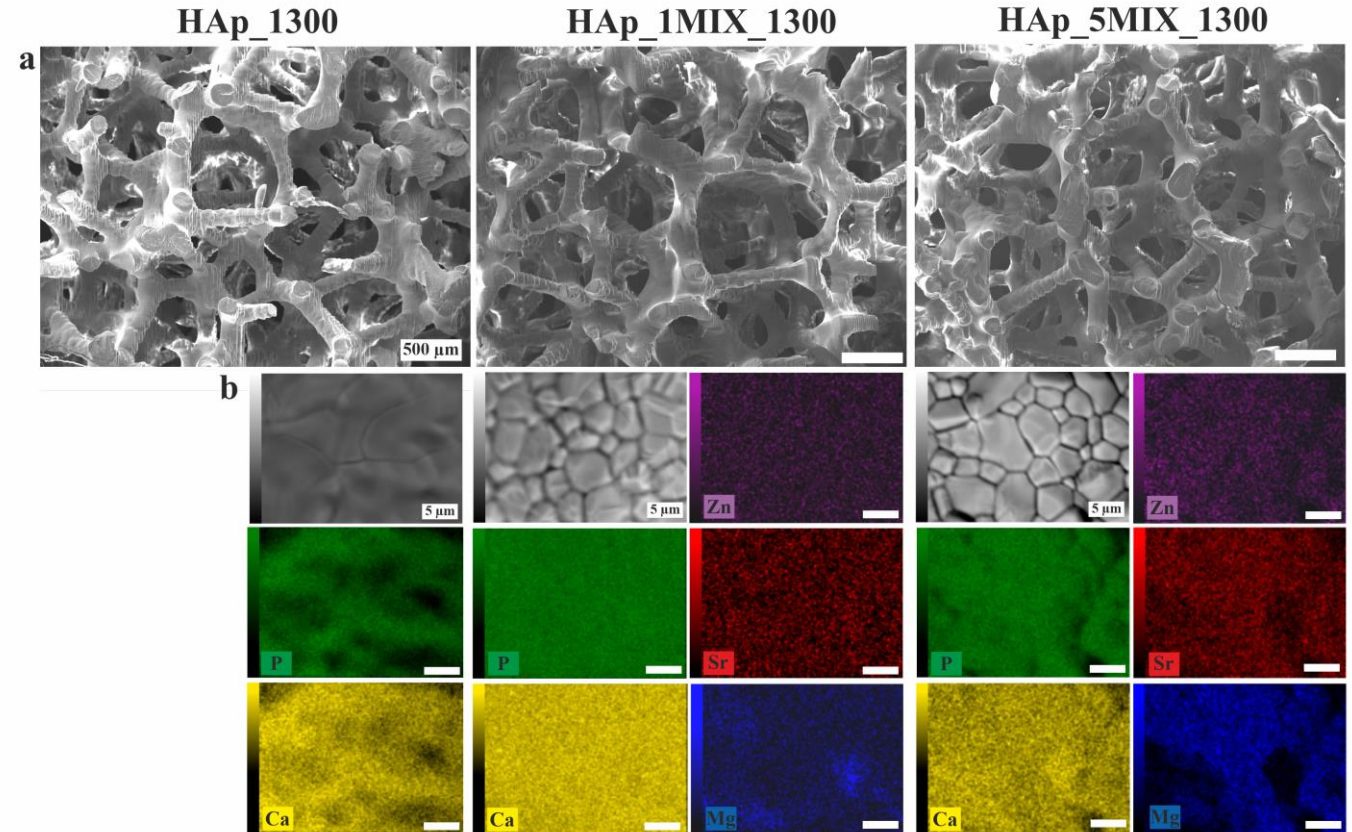
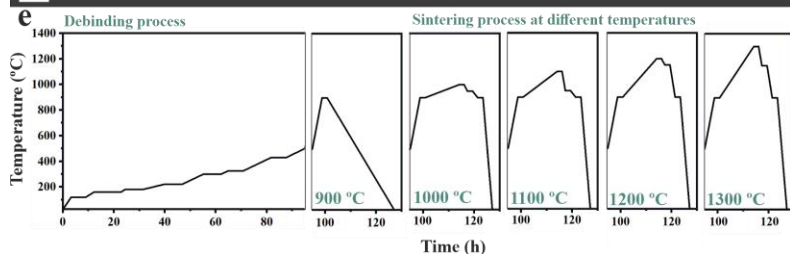
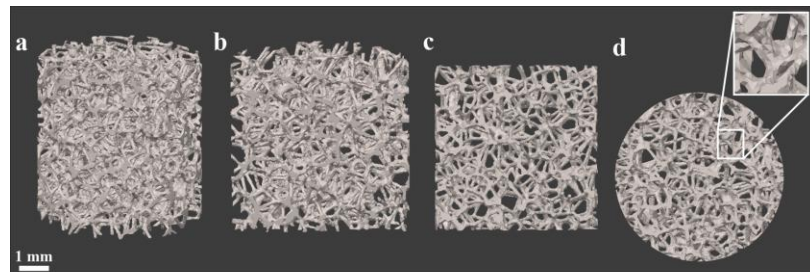
Vat photopolymerization of biomimetic bone scaffolds based on Mg, Sr, Zn-substituted hydroxyapatite: Effect of sintering temperature

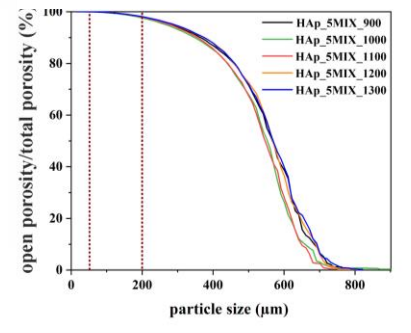
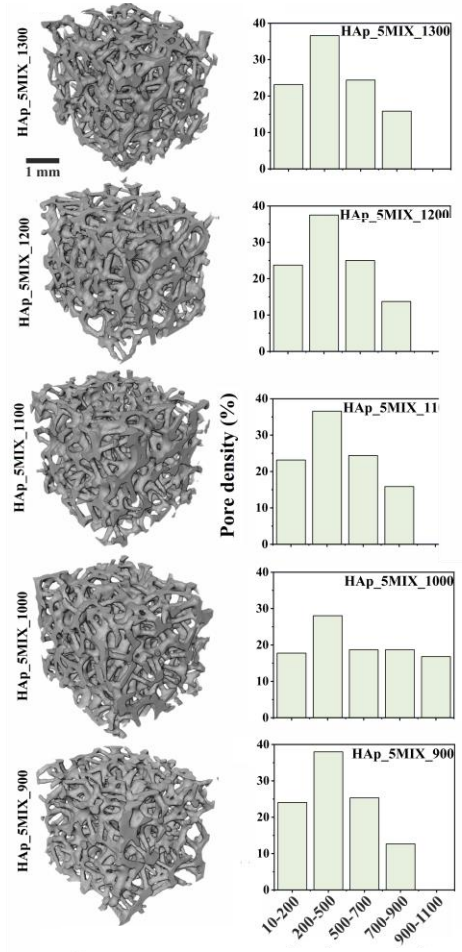
Antonia Ressler ^a ✉, Setareh Zakeri ^a ✉, Joana Dias ^b ✉, Markus Hannula ^c ✉,
Jari Hyttinen ^c ✉, Hrvoje Ivanković ^d ✉, Marica Ivanković ^d ✉,
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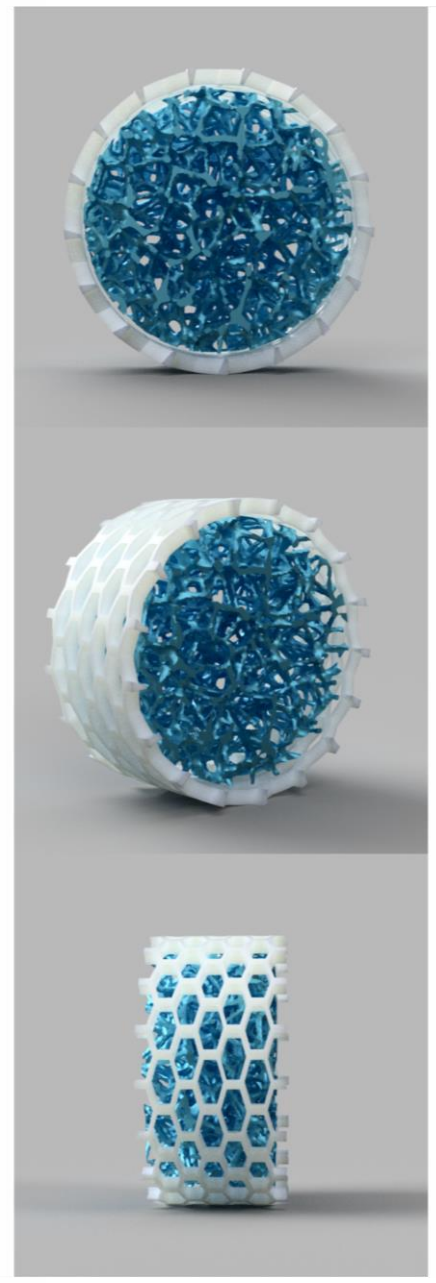
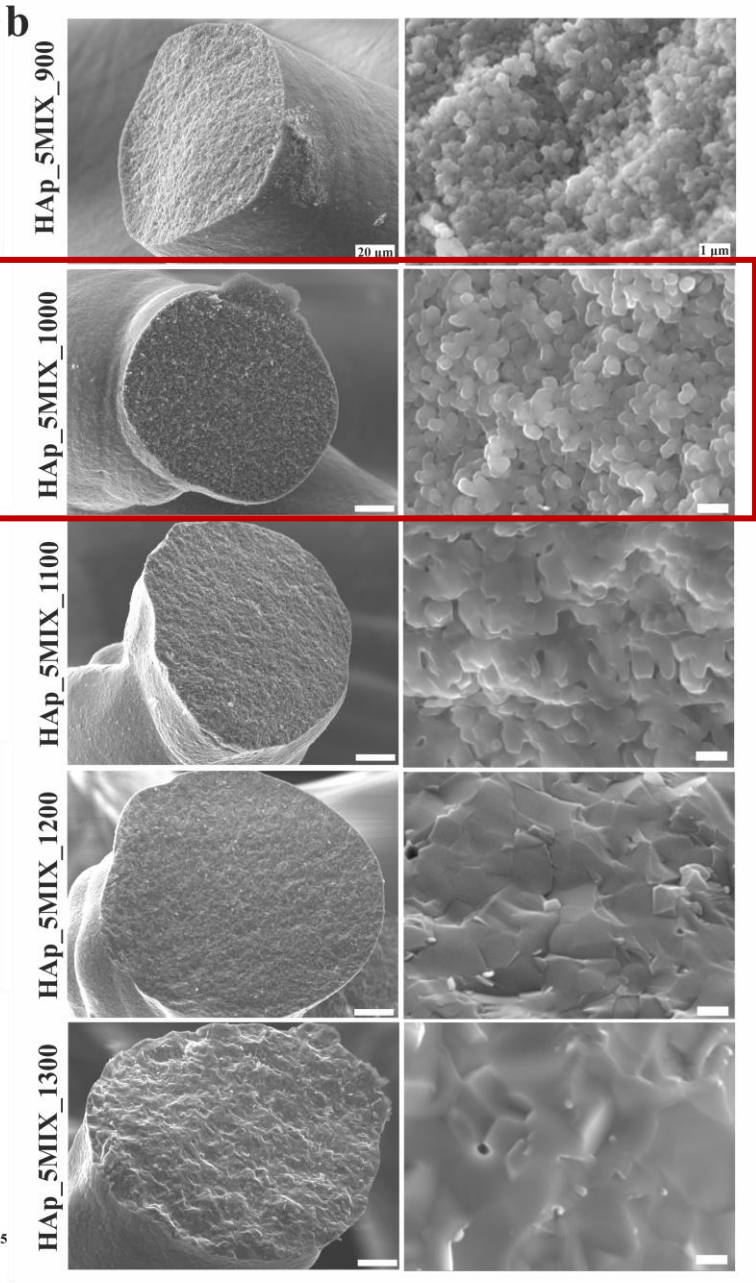
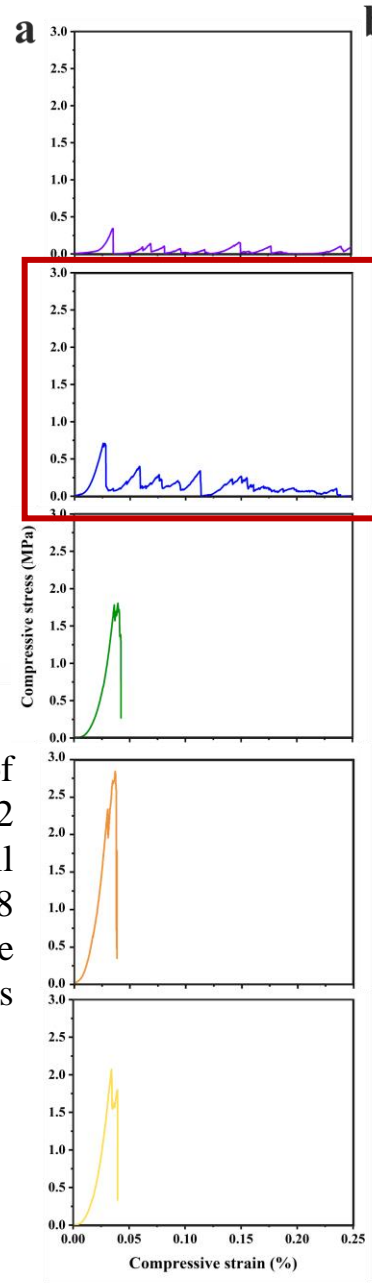
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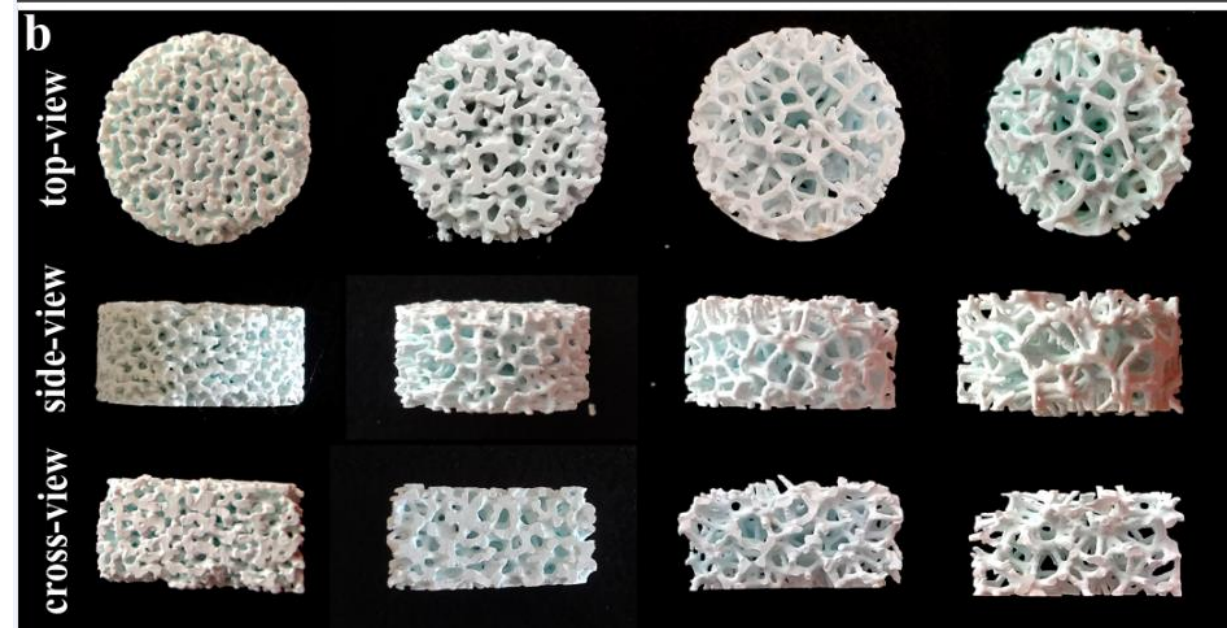
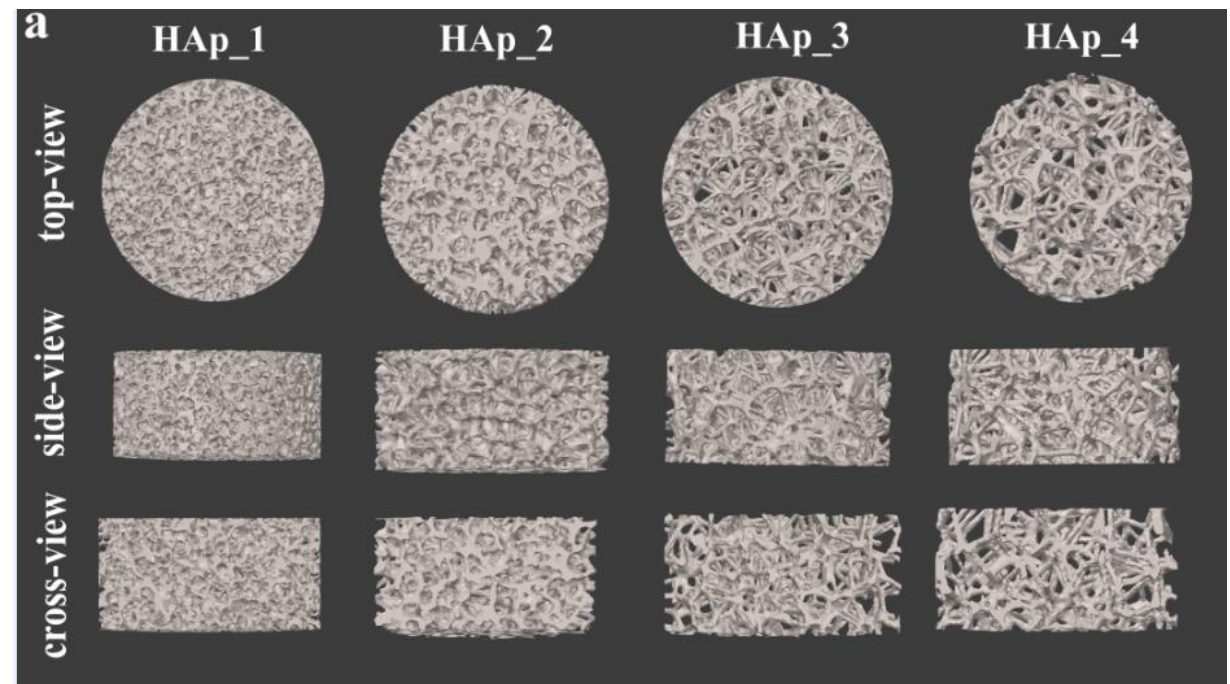
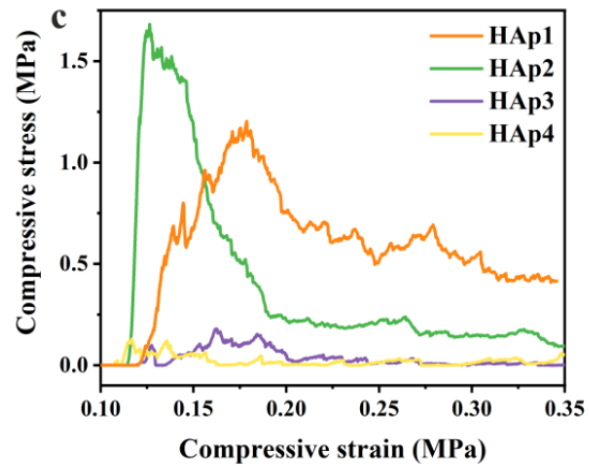
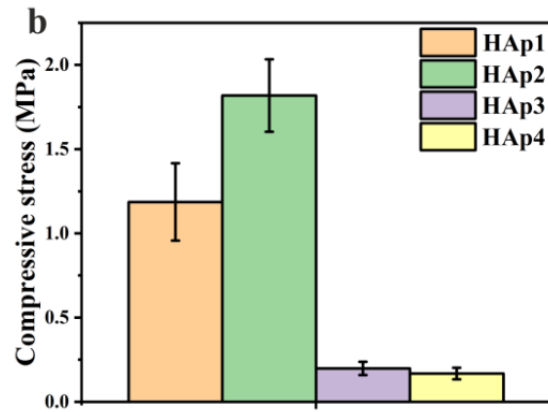


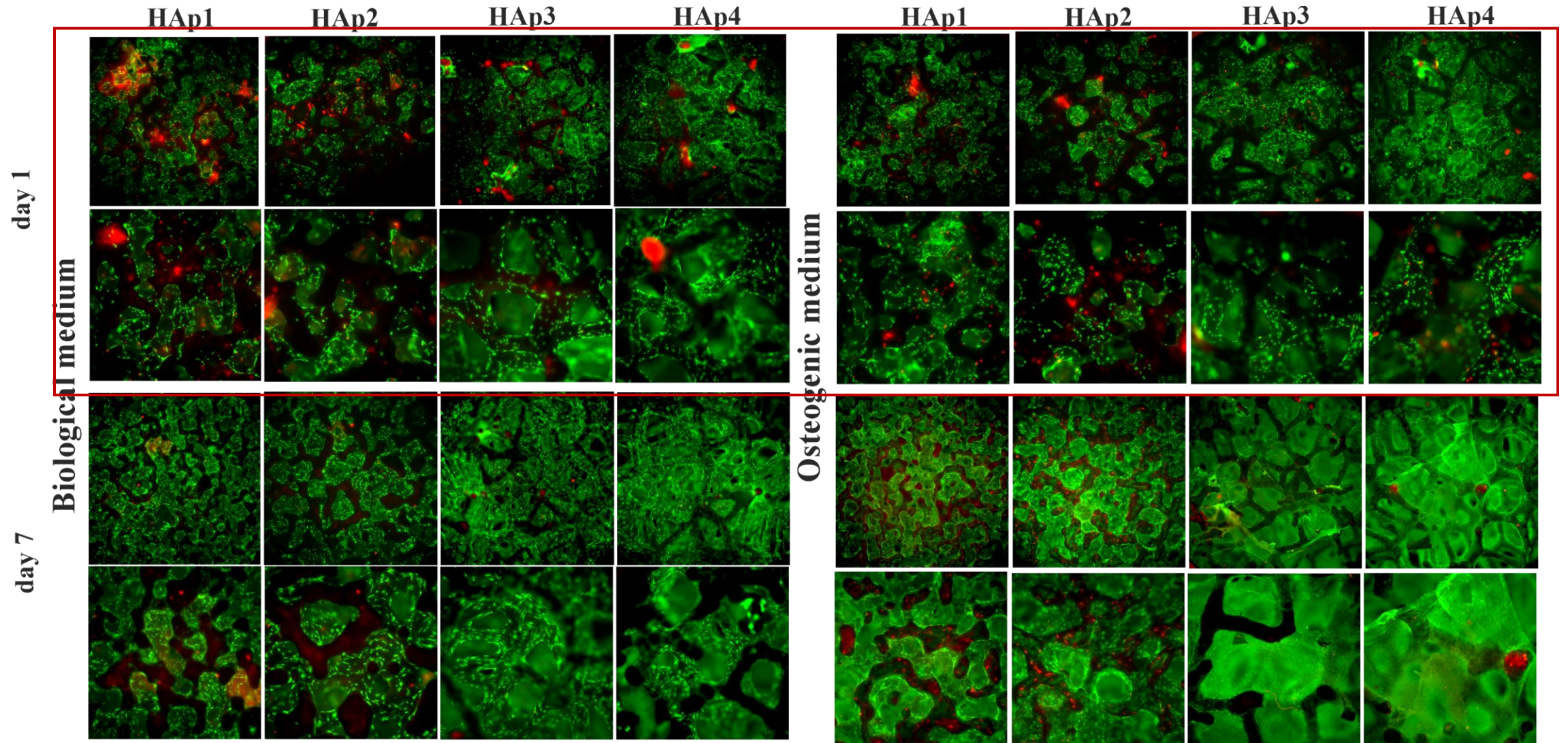


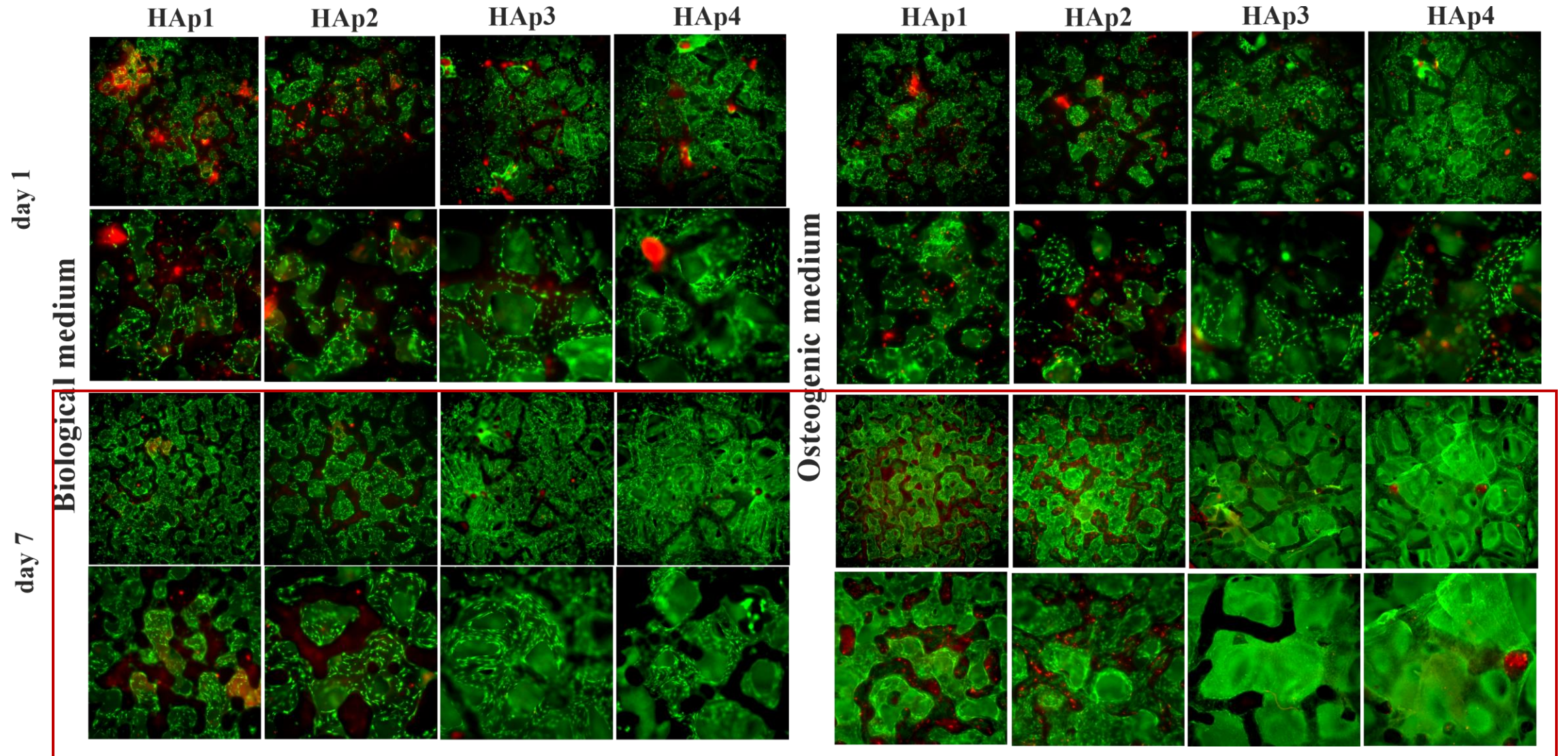
The total porosity of scaffolds was 76.24 ± 1.32 vol% and an average wall thickness of 217.03 ± 8.98 μm , closely resembling the morphology of cancellous bone tissue.



Effect of pore size and porosity

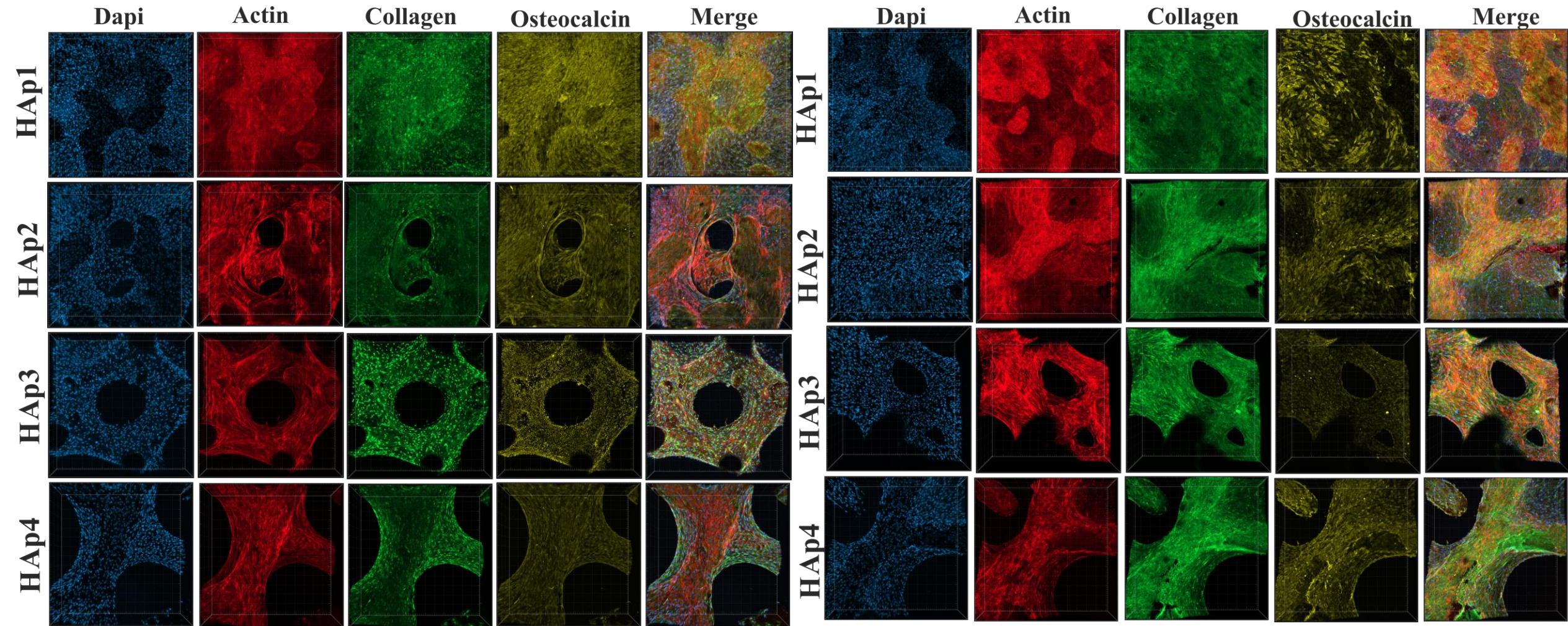


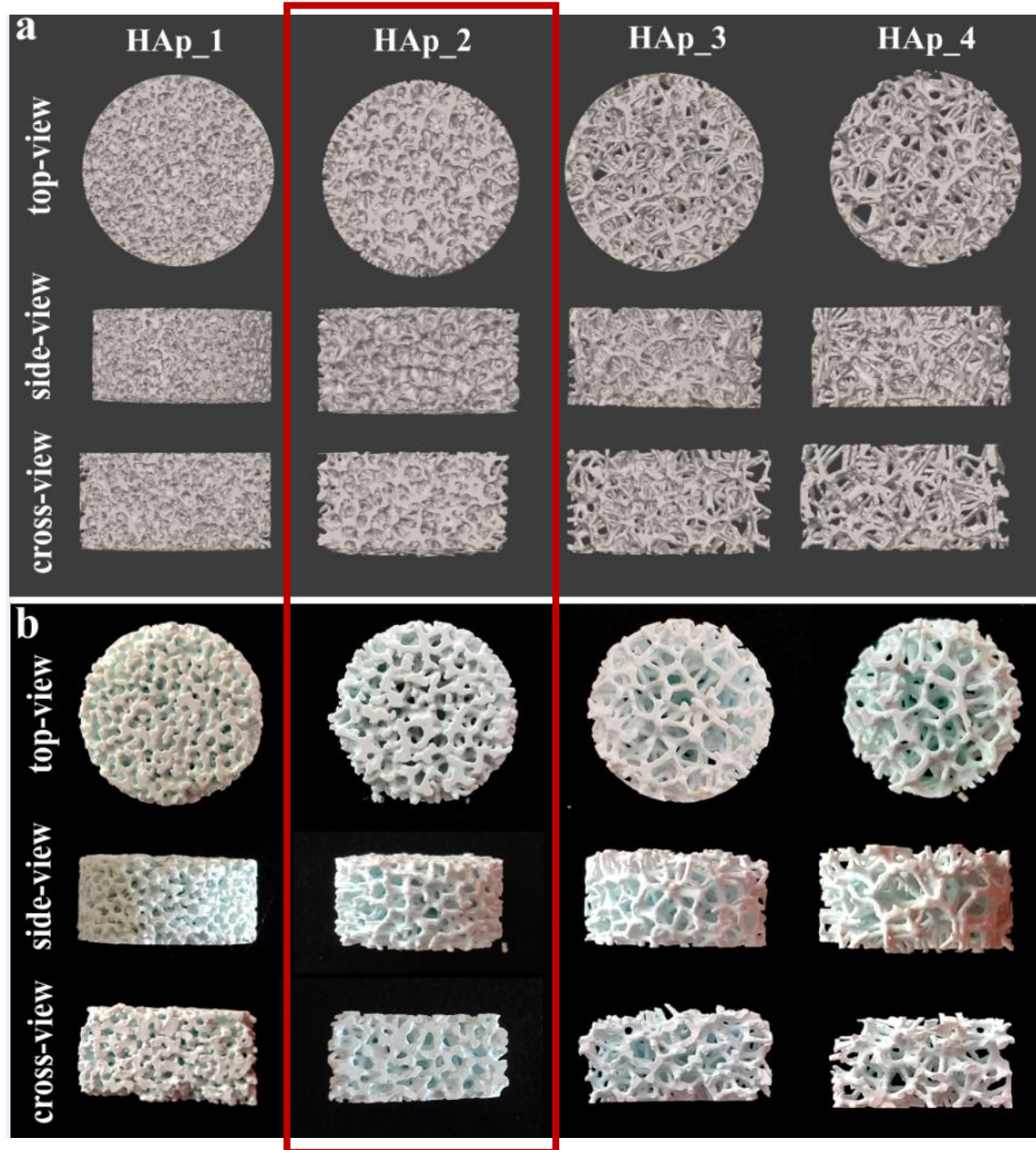




day 14

day 21

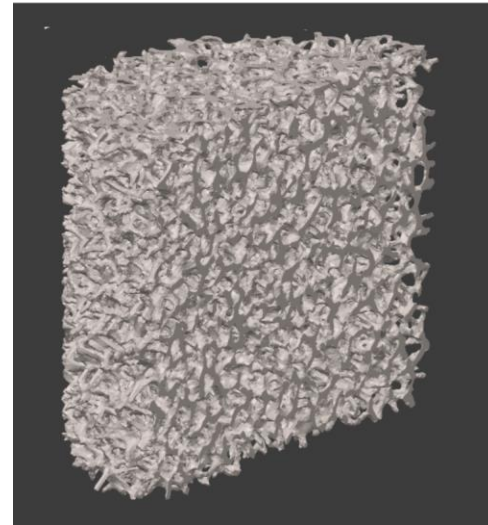




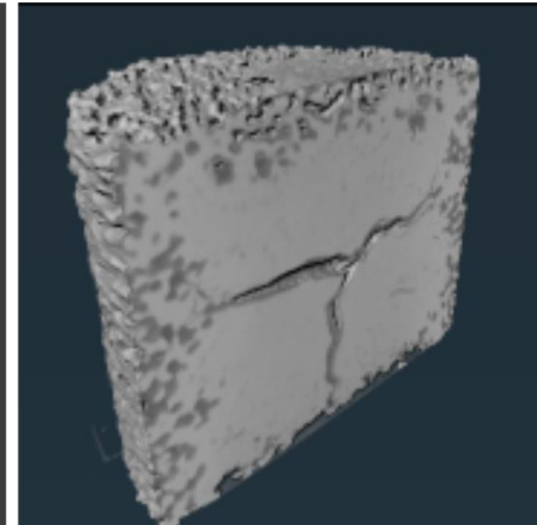
Cleaning challenge of porous scaffolds

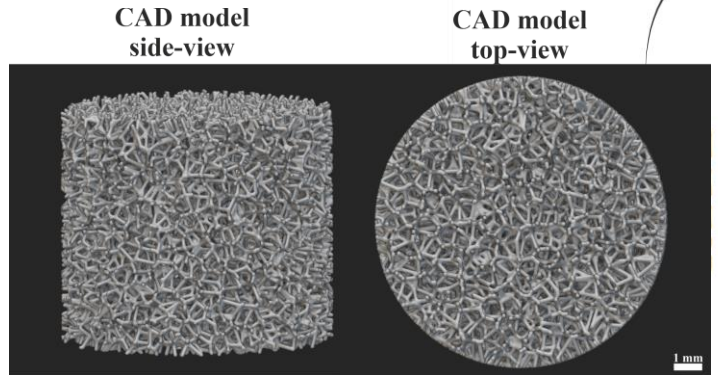
- porous structures where the interconnected pores are intentionally designed to remain uncured
- the uncured slurry in these porous regions can become intricately trapped between the cured layers, complicating the cleaning process
- effectively removing the uncured slurry from within the intricate and porous geometries of the printed structures becomes a critical task as the presence of residue within the structure can obstruct pores during sintering
- biomedical implants \longrightarrow pore characteristics are crucial for tissue integration and substance exchange.

**CAD model
cross section**



**micro-CT
cross section**





ultrasonic cleaning

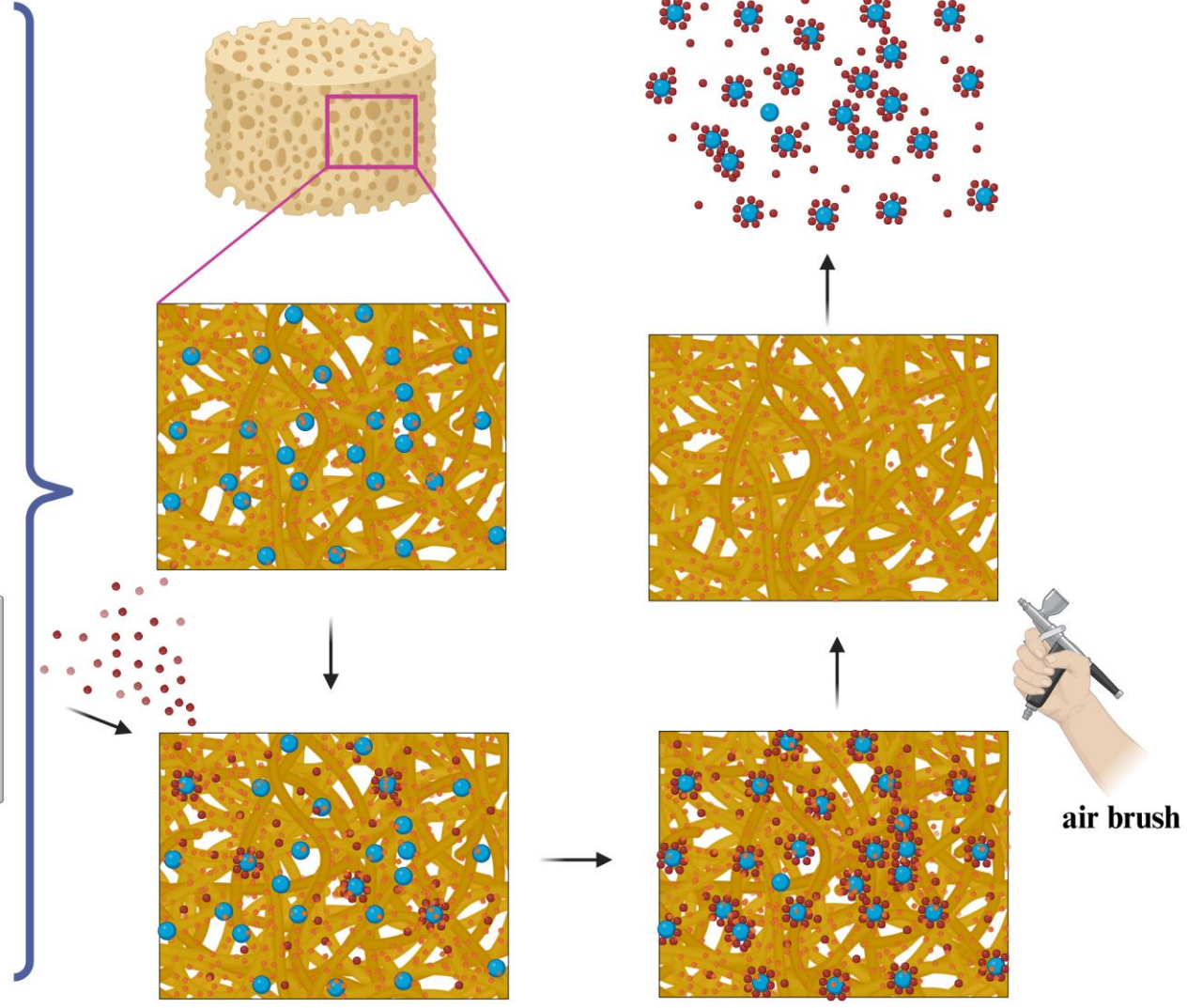


time points:
5, 15 and 30 min,
1, 2, 3 and 4 h

soaking cleaning

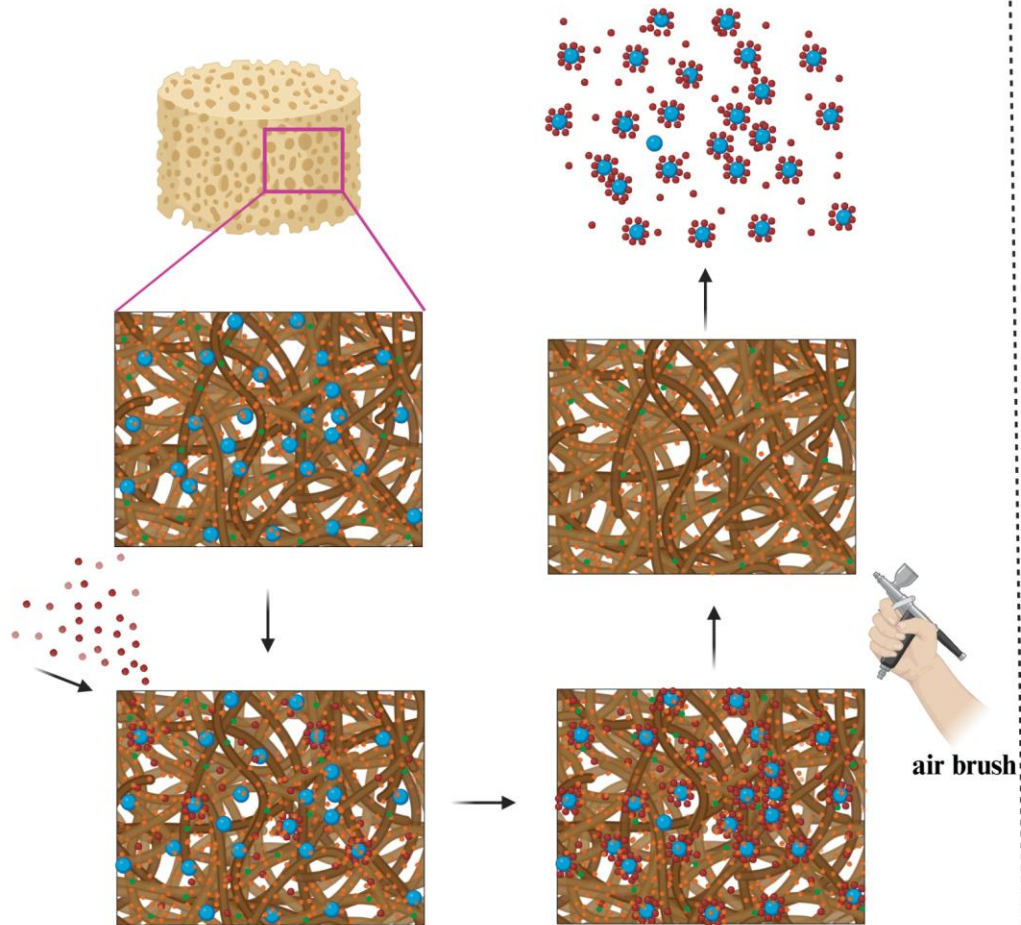


time points:
48, 72 and 96 h

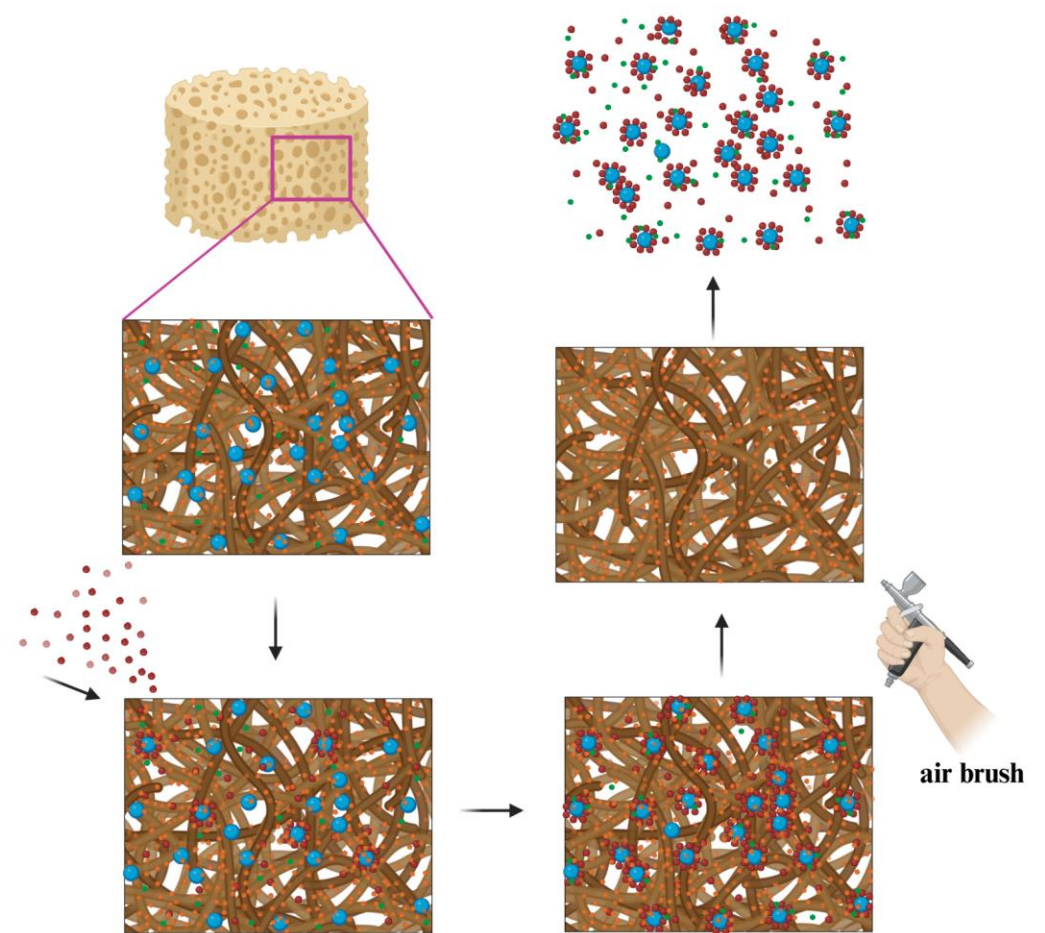







 polymerized scaffold part
  uncured polymer resin
  ceramic (HAp) particle
  LitaSol80 / DBE

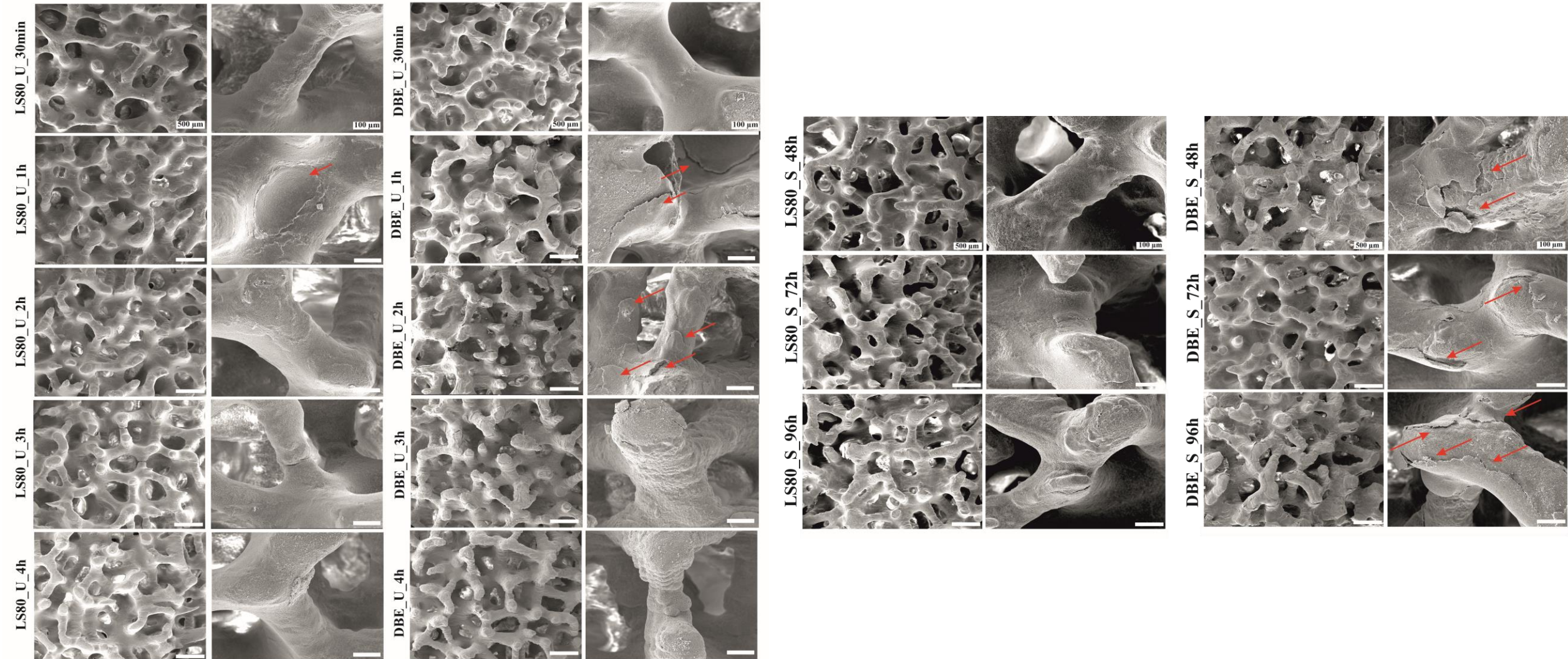
LithaSol 80 cleaning mechanism



DBE cleaning mechanism



 polymerized scaffold part
  uncured polymer resin
  ceramic (HAp) particle
  LithaSol80 / DBE
  additives and unreactive diluents



Conclusion...

Thank you for your attention!

antonia.ressler@tuni.fi