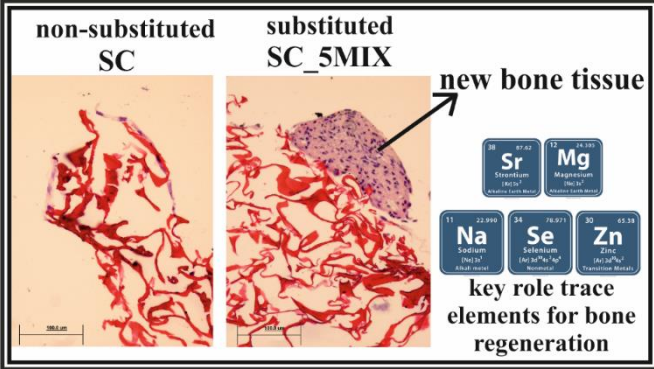


Cleaning strategies for 3D-printed porous scaffolds used for bone regeneration fabricated via ceramic vat photopolymerization

Antonia Ressler, Setareh Zakeri, Piie Konnunaho, Martin Schwentenwein, Erkki Levänen, Erkka J. Frankberg



Objective 1/WP1

mCaP precipitation, design of mCaP scaffolds using CAD and scaffold fabrication

scaffold CAD model

substituted mCaP CeraFab 7500 printer Collaboration with : LITHOZ

The mCaP scaffold properties according to the bone tissue engineering requirements:

- porosity: 50-90 %
- pore size distribution: 100-500 μm
- phase content: hydroxyapatite/tricalcium phosphate
- mechanical properties required for bone augmentation



Prof. Erkki Levänen



Dr. Erkkka Frankberg

Objective 2/WP2

In vitro and *in vivo* osteogenic properties of mCaP scaffolds

In vitro cell culture in **static** and **dynamic** conditions

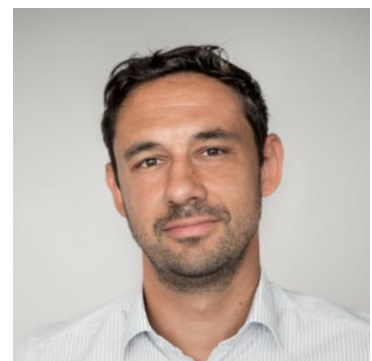
- live/ded assay, Cell Counting
- quantitative reverse transcription polymerase chain reaction
- immunocytochemical and immunohistochemical staining
- histological staining

In vivo characterization during three months in rats

- micro-computed tomography
- inflammation detection



Prof. Susanna Miettinen



Dr. Martin Schweintenwein



Objective 3/WP3

Obtaining a demonstration of personalized mCaP scaffolds in collaboration with Planmeca

- obtaining CAD design according to the real patient cases provided by Planmeca
- printing customized scaffolds on CaraFab 7500 using previously optimized printing parameters

Collaboration with : PLANMECA



Pontus Degerlund
PLANMECA

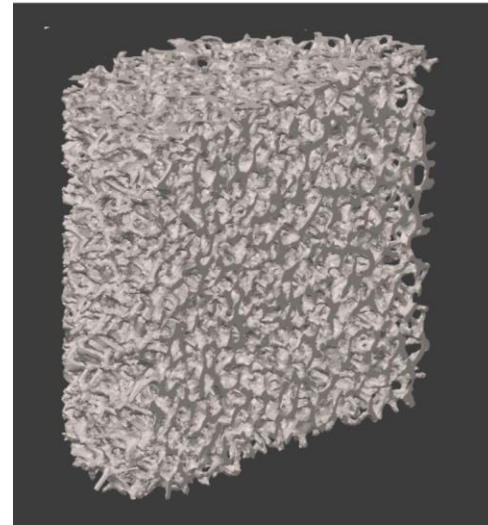


Dr. Antonia Ressler

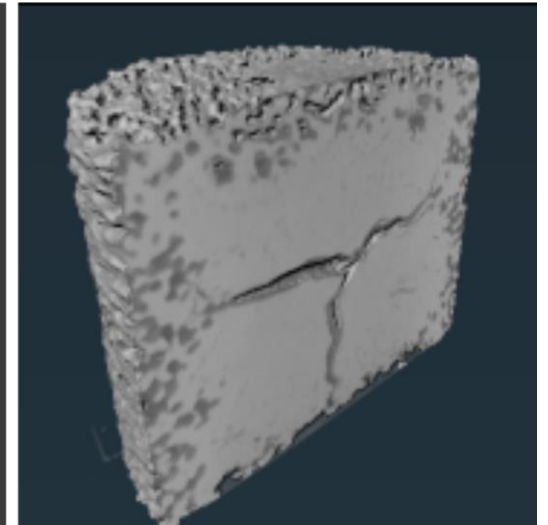
Cleaning challenge of porous scaffolds

- porous structures where the interconnected pores are intentionally designed to remain uncured
- the uncured slurry in these porous regions can become intricately trapped between the cured layers, complicating the cleaning process
- effectively removing the uncured slurry from within the intricate and porous geometries of the printed structures becomes a critical task as the presence of residue within the structure can obstruct pores during sintering
- biomedical implants → pore characteristics are crucial for tissue integration and substance exchange.

**CAD model
cross section**

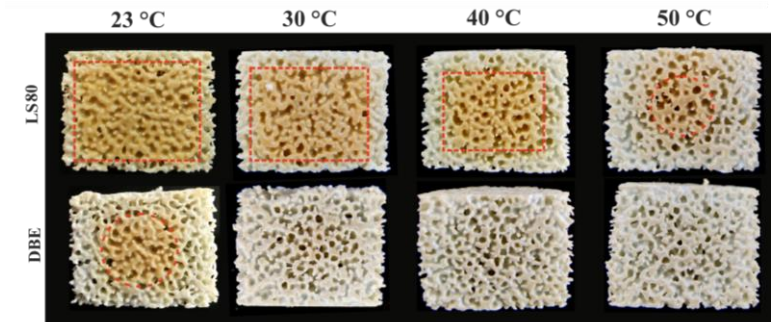
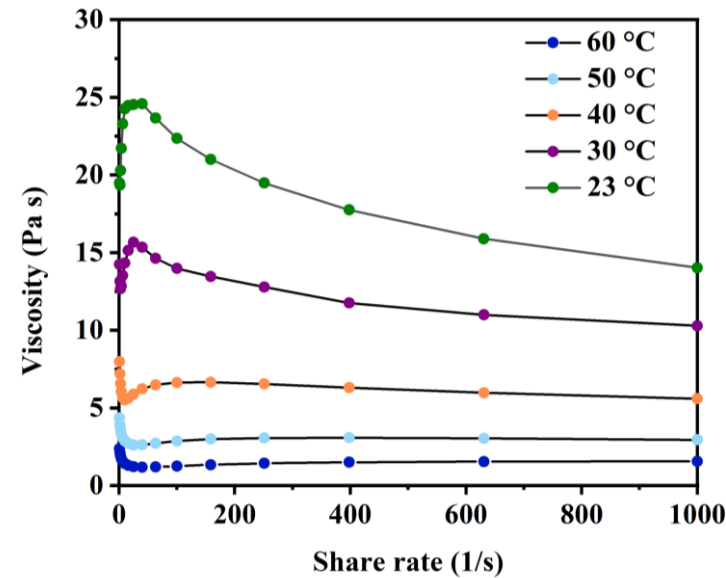


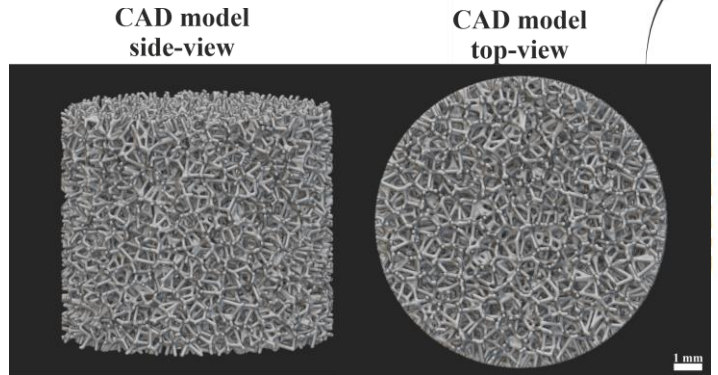
**micro-CT
cross section**



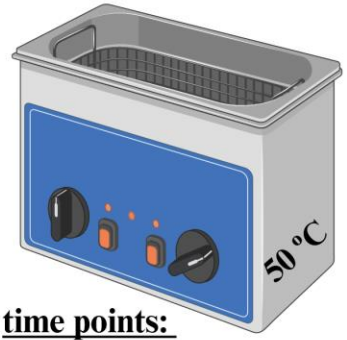
Preliminary experiments

- Increasing the temperature is effective in lowering viscosity and improving slurry flowability, leading to enhanced cleaning of the as-printed structures
- the difference in viscosity of slurry at 50 and 60 °C was small, leading to the exclusion of 60 °C from further studies to mitigate any risk of thermal polymerization of the ceramic slurry during the cleaning process





ultrasonic cleaning

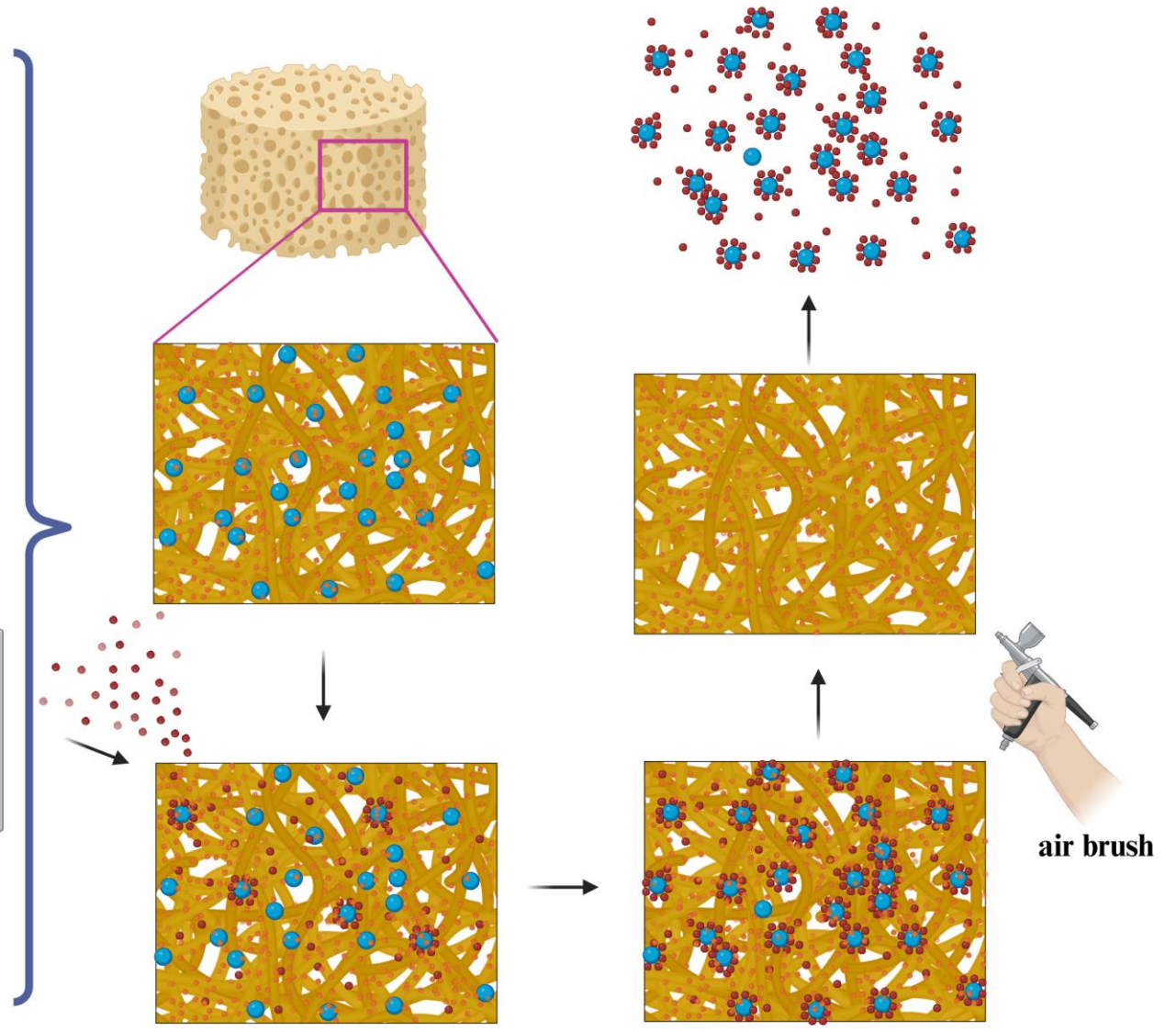


time points:
5, 15 and 30 min,
1, 2, 3 and 4 h

soaking cleaning

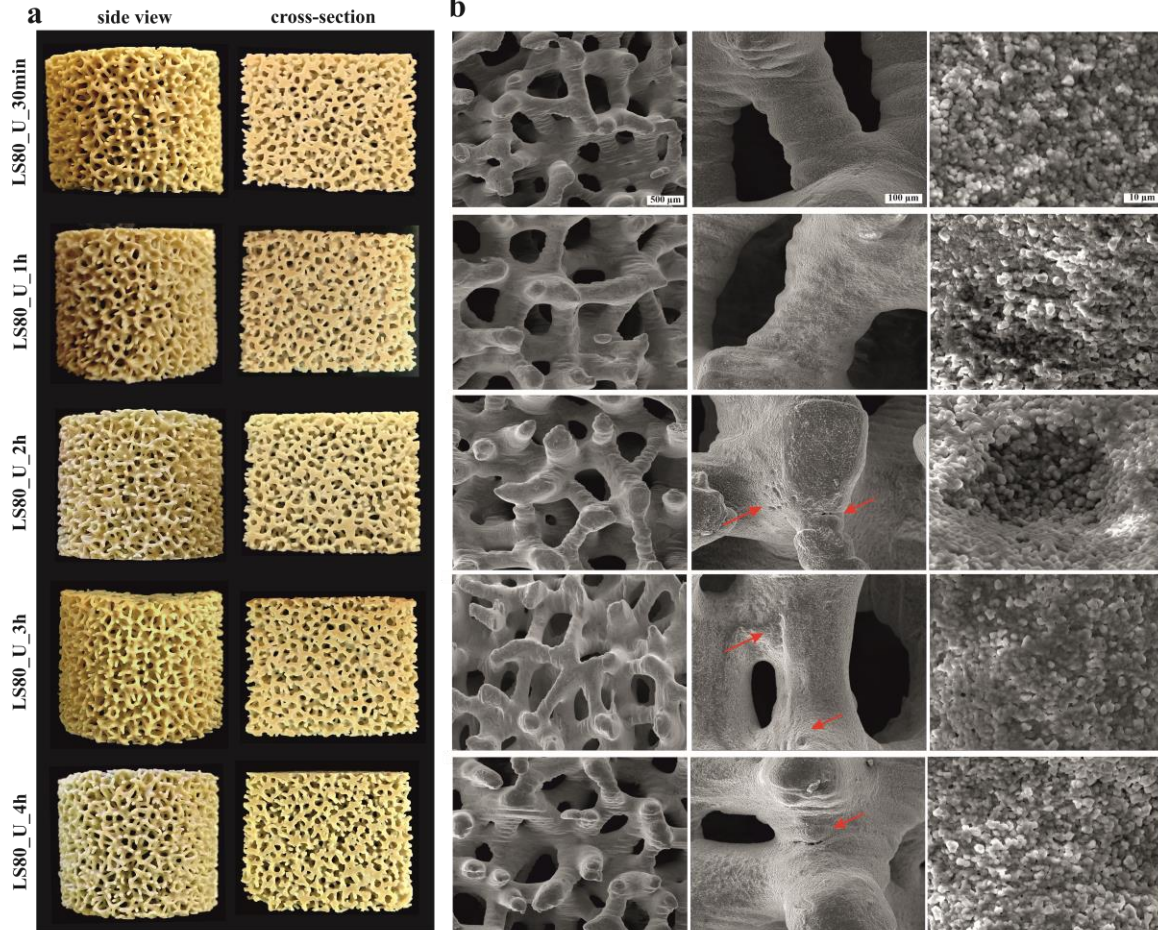


time points:
48, 72 and 96 h

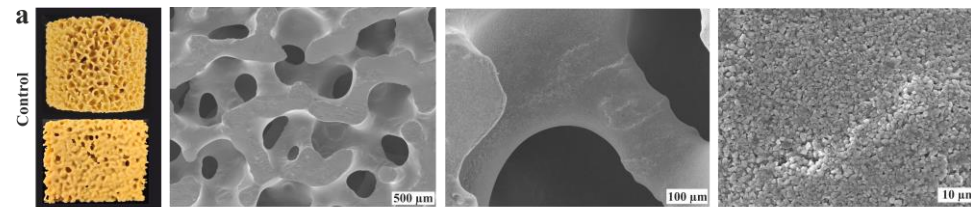
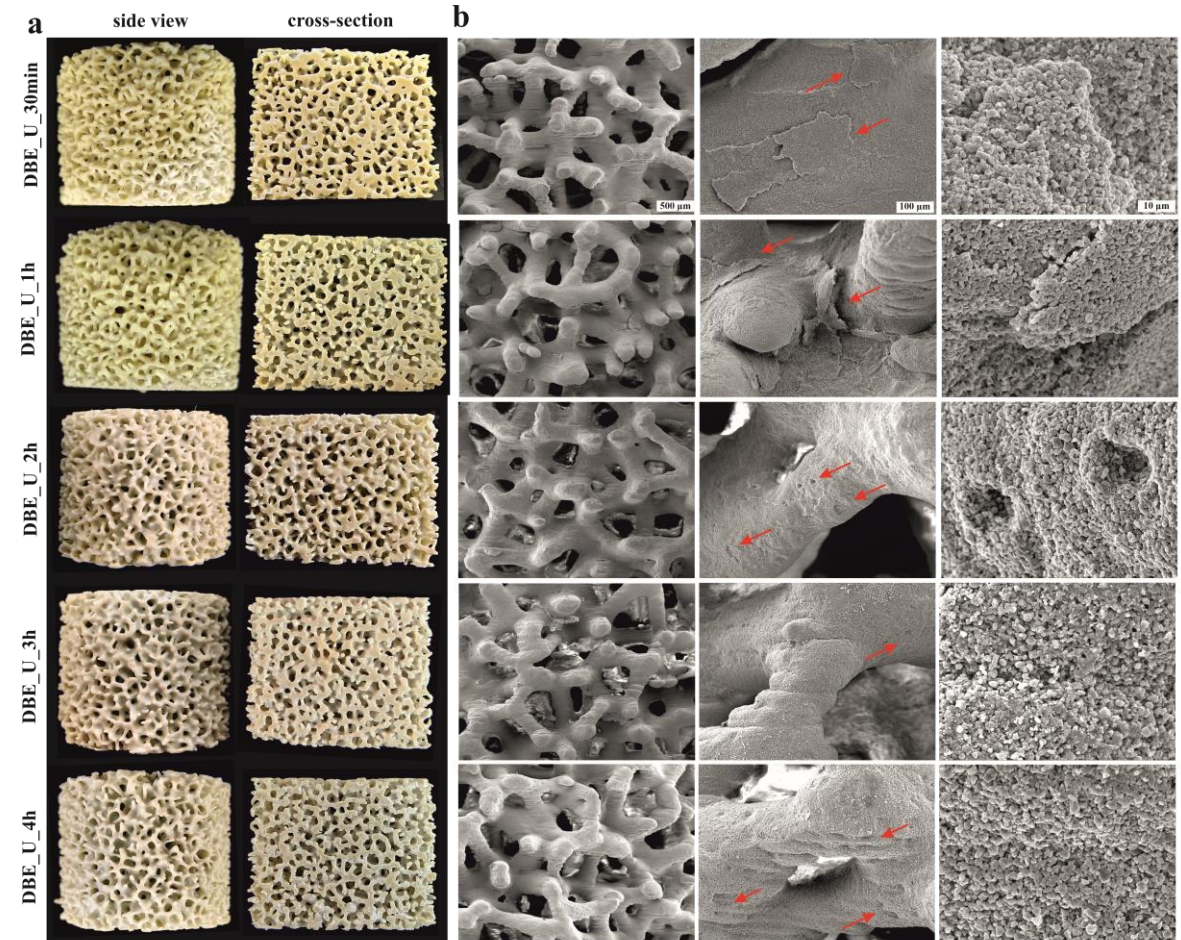


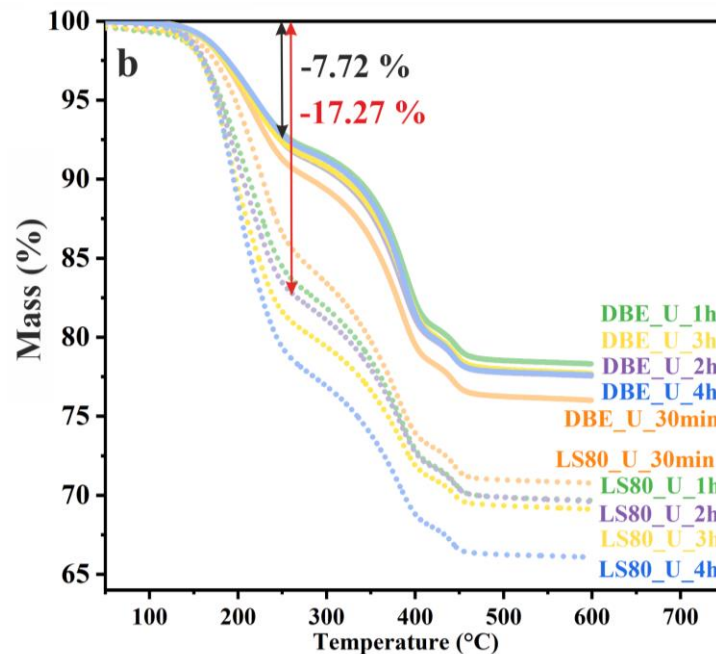
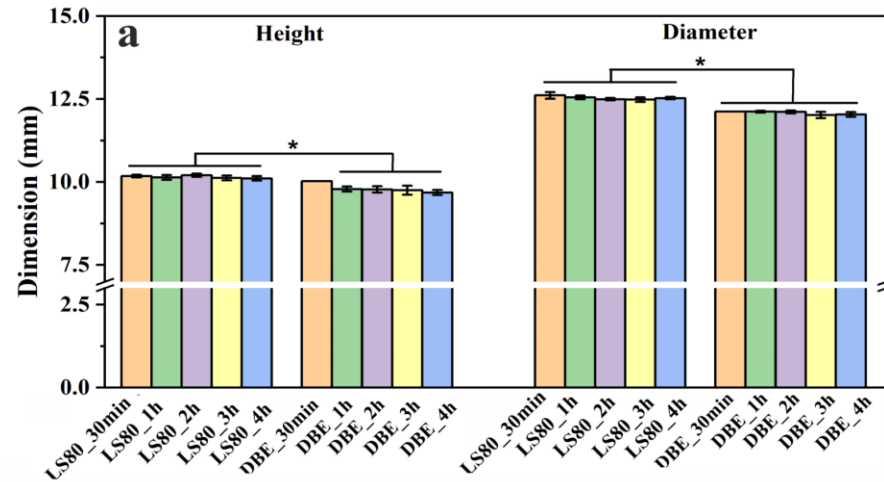
 polymerized scaffold part
  uncured polymer resin
  ceramic (HAp) particle
  LitaSol80 / DBE

LithaSol 80

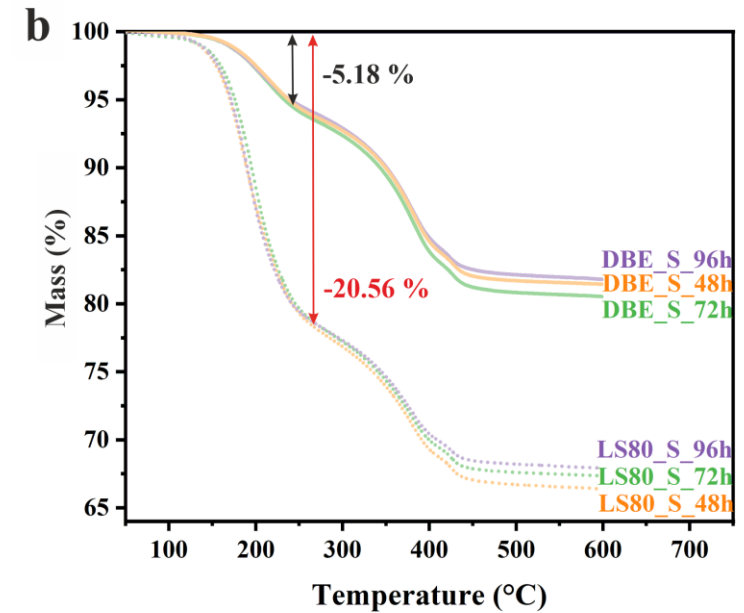
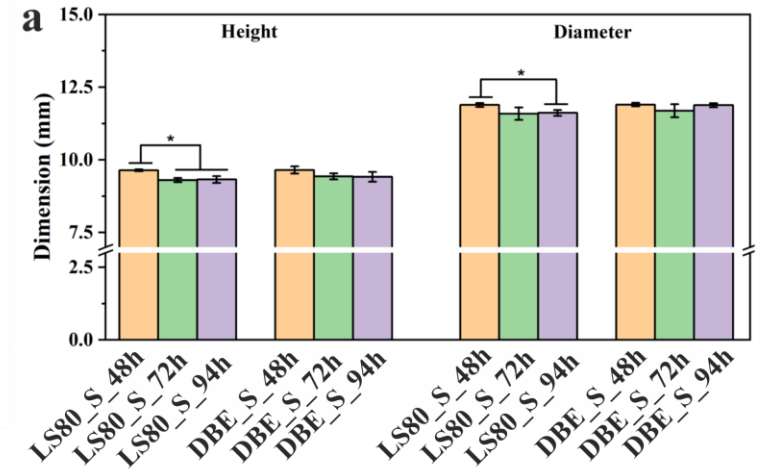
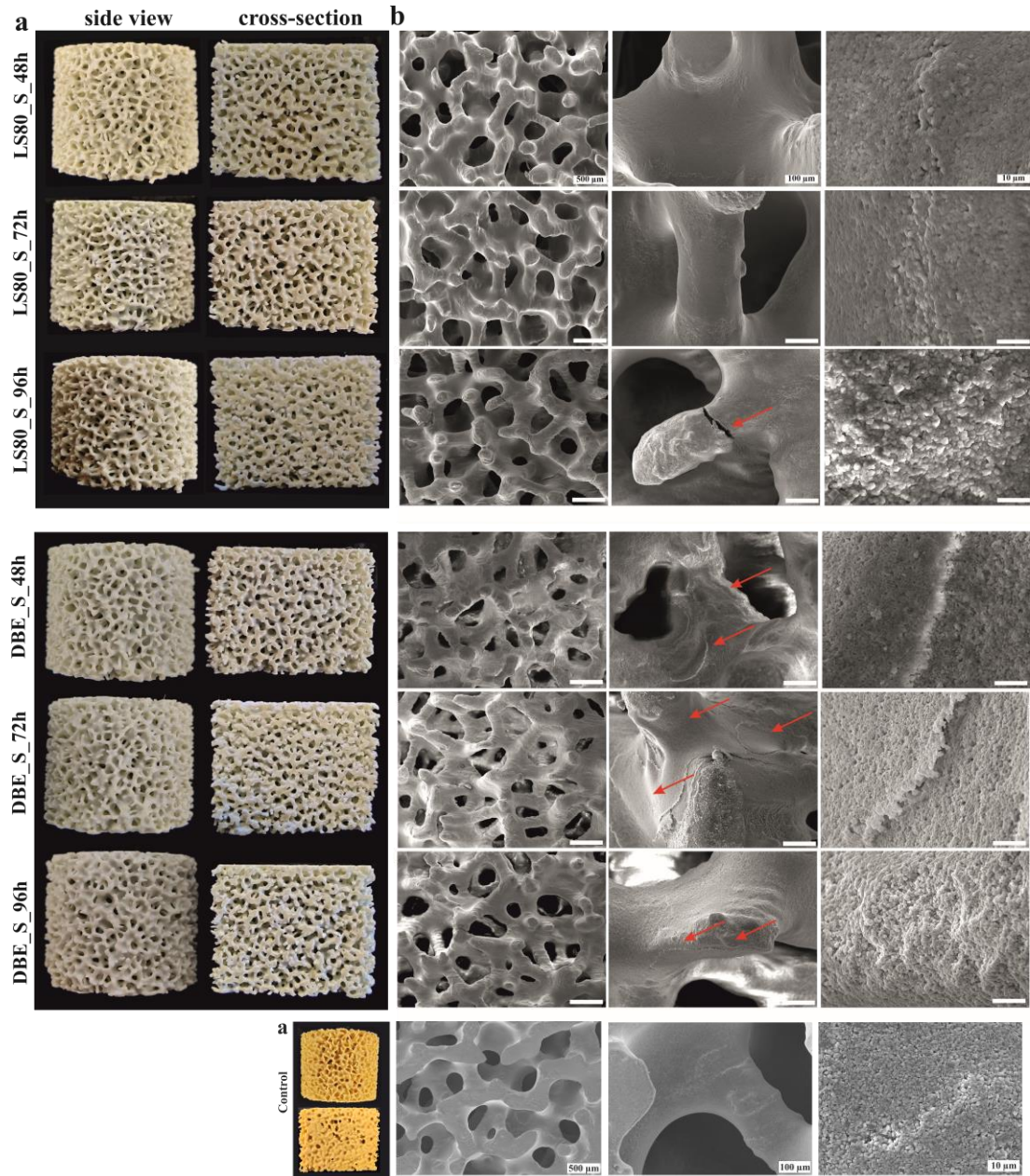


DBE

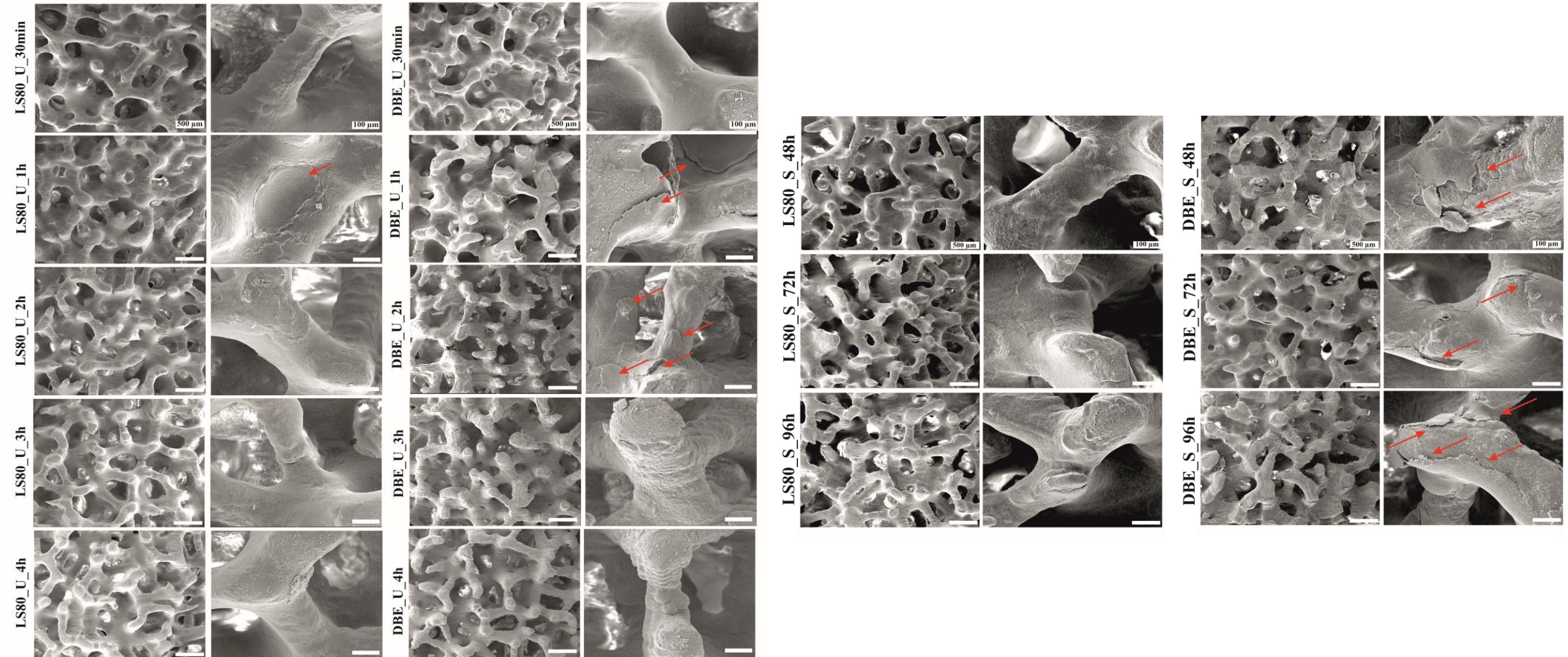


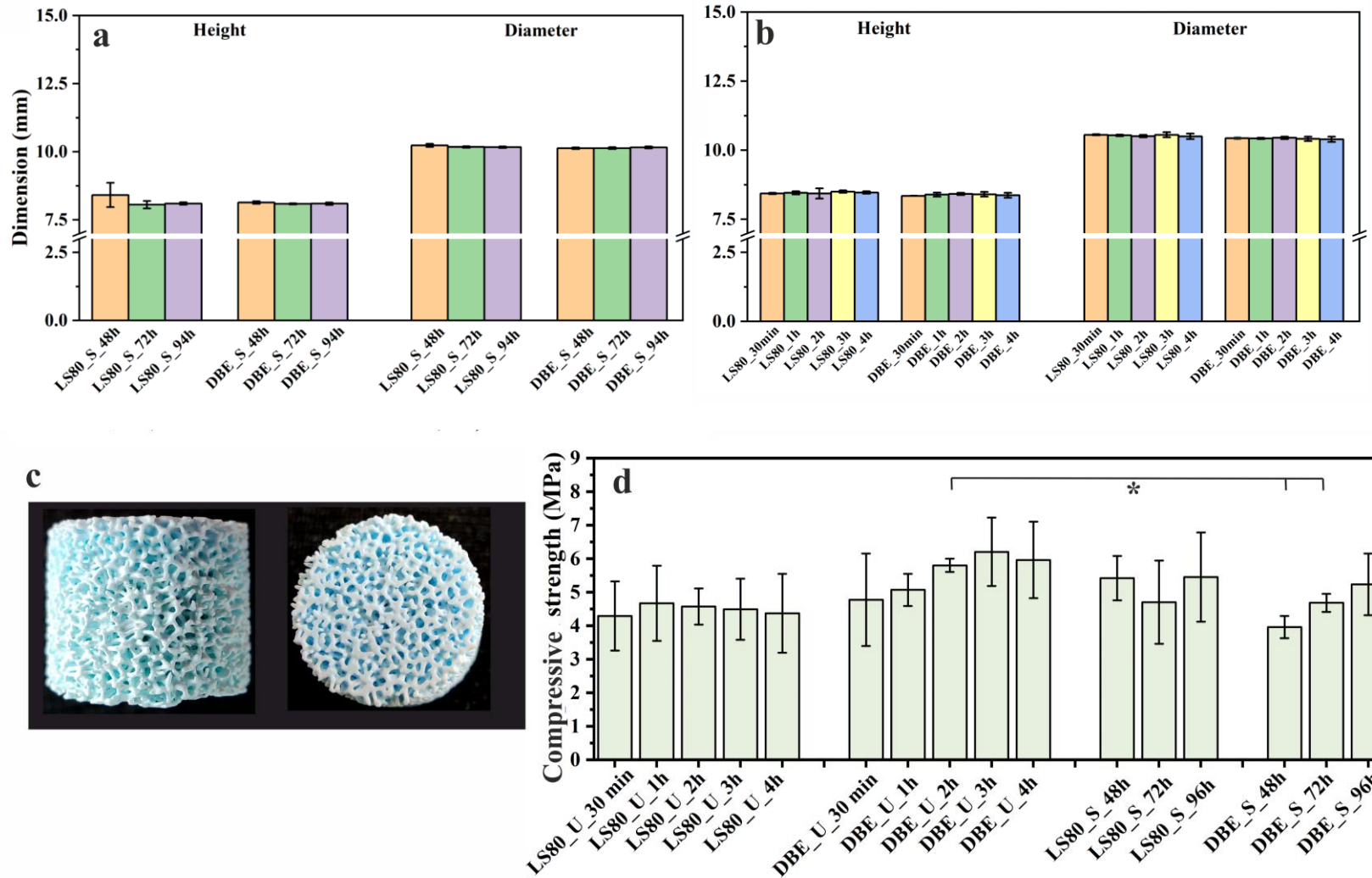


- mass loss started at approximately 150 °C, primarily attributed to the diffusion and evaporation of additives, unreactive diluents and uncured slurry
- the degradation of the major cured organic components initiated around 250 °C
- the significant contrast in the TG curves between scaffolds treated with LithaSol 80 and DBE primarily lies in the initial stage of weight loss
- the observed difference in total mass loss (14.15%) between samples treated with Lithasol 80 and DBE implies the potential occurrence of chemical debinding during cleaning with DBE. However, further detailed examination is required to provide conclusive evidence



Morphological characterization – sintered samples





Conclusion...

Thank you for your attention!

antonia.ressler@tuni.fi